A SIMPLE POLARIZED-BASED DIFFUSED REFLECTANCE COLOUR IMAGING SYSTEM

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ABSTRACT
A simple polarized-based diffuse reflectance imaging system has been developed. The system is designed for both in vivo and in vitro imaging of agricultural specimen in the visible region. The system uses a commercial web camera and a halogen lamp that makes it relatively simple and less expensive for diagnostic research and teaching. The system has been used to demonstrate the difference between a yellow colour of a diseased cassava leaf and that of a senescence cassava leaf qualitatively using diffused reflectance images. Predicting the area of the sample using a method of counting dark pixels is presented. This method avoids complex and more computational power required by edge detection algorithms. The performance of the suggested method can be seen for 50 samples of leaves. This suggest that polarized diffused reflectance image lends itself to extraction of physical information.

INTRODUCTION
Among various diagnostic optical techniques, reflectance spectroscopy is considered to be one of the powerful techniques in a large variety of non-destructive, non-intrusive, fast and real-time applications in many fields, such as agriculture, medicine and environmental monitoring (Curran et al., 1992; Batten, 1998; Cheng and Boas, 1998; Foley et al., 1998; Young-Ah et al., 1999; Cozzolino et al., 2001; Ji et al., 2002; Cozzolino and Moron, 2003; Qin and Lu, 2008; Zhu et al., 2006; Stelzle et al., 2010; Stelzle et al., 2011). The ability of reflectance technique to be used in the mentioned fields is critically useful, because there is no or little sample preparation, which in effect reduces human error, time and cost. Most material surfaces act like a dielectric boundary such that the surfaces scatter and absorb light (Born and Wolf, 1965). The scattering may result from specular and/or diffuse reflection. The specular component is a surface phenomenon, where the Snell’s laws are obeyed and contains’ information about the surface topology, such as texture. For uneven surfaces the specular components are concentrated in a compact lobe in the vicinity of the specular direction. This concentration of light intensity causes highlights in bright image scenes. These strong highlights cause problems for intensity related analysis thus producing erroneous results (Nayar et al., 1993; Bhat and Nayar, 1995). So these specularities are often eliminated in image processing, when physical
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and chemical information of the material is required.

The diffuse reflection results when light penetrates through a surface and undergoes multiple scattering and re-emerges at the surface from the medium. The back-scattered light is distributed in a wide range of directions within the medium, thus becoming depolarised relative to the incident light, giving an image a dull appearance (Nayar et al., 1993). The spectral dimensions of diffuse reflection are generally governed by the molecular makeup of the material medium, and so much of the physical and chemical information about a material can be obtained from the diffuse reflected part of the reflection.

For both synthetic and natural materials, diffuse reflection spectroscopy has been used, in both basic and applied research, for quantitative and qualitative analysis of various materials, (Kienle et al., 1996; Doornbos et al., 1999; Ji et al., 2002; Fabbri et al., 2003; Dean et al., 2008; Yu et al., 2008; Stelzle et al., 2010; Stelzle et al., 2011). In biological and medical research, the study of respiratory enzymes in vivo has become possible due to diffused reflectance. Amount of glucose and quantification of tissue absorption and scattering in vivo can be researched into using diffused reflectance (Cameron and Li, 2007; Yu et al., 2008)

Also, polarized light-matter interactions have made polarized-based optical techniques to have potential applications (MacKintosh et al., 1989; Schmitt et al., 1992; Jacques et al., 2000; Ramella-Roman et al., 2002; Arimoto, 2007; O’Doherty et al., 2007; Cameron and Li, 2007; Stelzle et al., 2011). Polarimetric dimensions are governed by sample geometry and surface properties and can vary substantially with viewing geometry, but spatial and spectral signatures, are reasonably stable with viewing geometry. However, the advantages of polarization are that polarized light reduces the degrees of freedom of the reflected lights and eliminates the polarization memory of specular reflected light (MacKintosh et al., 1989), when cross polarizers are used. Specular reflection can be eliminated, when information about the surface properties and image acquisition geometry are not required. Whereas polarimetric signatures present an attractive prospect for increasing the dimension of sensed data, they also present new collection, modelling, and analysis challenges. The depth of penetration of a polarized light depends strongly on the optical properties of the medium at each present wavelength (Liu et al., 2005).

Most of the polarized-based reflectance imaging systems described in literature (MacKintosh et al., 1989, Liu et al., 2005) employ specialized equipment that is not easily accessible to most researchers. With the advancement in technology, commercial web camera (web-cam), which are fast, cheap but reliable imaging systems and making use of cheap Complementary Metal Oxide Semiconductor (CMOS) are now available.

In this study, we present a low cost and simple polarized-based diffuse reflectance imaging system (PBDRIS) that uses a web-cam. The relevance of this instrument to measure diffuse reflectance is illustrated with infected African cassava mosaic diseased leaves and non-infected cassava leaves.

MATERIALS AND METHODS

The general arrangement for our polarized-based diffused reflectance colour imaging system is illustrated in Figure 1. A photograph of the complete instrumentation is shown in Figure 2. Light source for diffused reflection is a 30 W halogen lamp housed in cooling vents that allow convection currents to bathe the lamp with cooler air during operation.

The entire system is housed in a wooden frame which was designed by us and built by the University carpentry division (Figure 2a). A well dried red wood of dimension 1.5 x 1.5 cm was used to form the wooden frame of 12 x 12 x 21 cm as the outer dimensions. The actual sample chamber, rectangular in shape, 9 x 9 x 12.5 cm was enclosed with a black card-board as well as its floor. An upper chamber housed the major electronic components; the web-cam, light...
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source and its power supply (step-down transformer), and the dimmer (Figure 2b), of the system. The electronic system is controlled by a personal computer (PC, Dell), which is used for data acquisition, storage and image analysis.

The lamp is powered externally by a 12 VDC step-down transformer from the mains (240 V, 50 Hz). Attached to the light is a dimmer that controls the light intensity in relation to the sample. This light intensity is monitored by

Figure 1: Schematic view of the completed polarized-based multispectral imaging system

Figure 2: System instrumentation: (a) complete system with the sample chamber (lower) and the upper chamber (fully covered) which holds the electronics. (b) Uncompleted system instrumentation showing the upper chamber which holds the web-cam, light source, step-down transformer and dimmer.

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A light intensity histogram, an algorithm that was developed by us using MATLAB software (Matlab 7.10.0, 2010).

A metallic spherical reflector lining the inner part of the lamp-house assists to direct the greatest possible level of luminous flux into the collector lens system for delivery unto the sample. The lamp’s position in relation to the spherical reflector and collector optical axis can be adjusted using a translating screw. The spectral range of the light source is from 400 nm to about 900 nm. Figure 3 shows the emission spectrum of the light source as was measured with an Ocean Optics USB 4000 Spectrometer. The spectra broadness of the light source makes it appropriate for reflection imaging.

A commercial web camera (web-cam) with USB 2.0 (Universal Serial Bus) interface is used as the colour (Red, Green and Blue) imager. The web-cam has 640 × 480 (307,200 pixels = 0.3 Mega pixels) absolute maximum resolution and each Red, Green and Blue channel has 8 bit intensity depth. The size of the CMOS (Complementary Metal Oxide Semiconductor) sensor of the web-cam is 4.86 mm ×3.64 mm. The viewing area of the imager has been set to 16 x 12 cm². Hence, the system has 1600 pixels per square centimeter pixel density and 10.9 times magnification. The web-cam is capable of acquiring 15 frames per second when it is at its maximum resolution.

Because the system is mainly intended to image diffuse reflection, linear polarizer and analyzer (NT43-781, Edmunds Optics) have been used to eliminate the specular reflection. The linear polarizer was placed in front of the light source and the analyzer placed in front of the imager. The polarizer and analyzer were mounted in such a way that the polarization planes are totally crossed.

**Imaging Procedure**

From the PC, our developed MATLAB code was used to control the electronics to aid the data acquisition. The image acquisition process, using the imaging system, is shown as a flow chart (Figure 4). The intensity distribution of the viewing area for a white paper is measured. This spatial domain of the light intensity distribution is used to normalize sample images in order to compensate for the error due to uneven light distribution from the source. When the background image is subtracted from sample image, features of the sample can be easily extracted.

![Figure 3: Emission spectrum of the light source in the system: measured using Ocean Optics USB 4000 Spectrometer.](image-url)
In the event that many samples of different areas are to be compared, other than the correction of the uneven distribution of the light intensity, effect due to the area should be corrected. In order to eliminate the area dependence an edge detection algorithm was used to calculate the area of the samples. The method of counting dark pixels and predicting the area of the sample was studied. In this suggested method, background subtracted image is considered.

The total number of zero intensity (dark) pixels was subtracted from the total number of pixels and that number is a good estimate for the area of the sample. Our developed imaging system was also used to image severely infected African mosaic diseased cassava (ACMD) leaf, mildly infected, a healthy cassava leaf (control) and a senescence cassava leaf.

**RESULTS**

The intensity distribution of the viewing area for a white paper measured is shown in Figure 5. The positions of the light source and the camera are marked in the figure. From Figure 5, the normalized intensity of the top graph, which is depicting the horizontal cross-section of the image plane taken from left to right decreases.

This shows the brightest position of the light source in the imaging plane. Likewise, the left graph, depicts the normalize intensity along the
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vertical cross-section of the image plane. Both graphs indicate non-uniformity of the light source in the image plane.

The method of counting dark pixels and predicting the area of the sample yielded a good estimate for the area of the sample. Hence, by using this method, complex and more computational power that consume edge detection algorithms was avoided. The performance of the suggested method can be seen for 50 samples of leaves in Figure 6.

Figure 7 shows the images of classes of healthy and diseased leaves imaged with the system. The classes of the cassava leaves are made up of healthy green, mildly mosaic infected, severely mosaic infected and healthy senescence cassava leaf.

Figure 8 shows an example of how the images of the cassava leaves were acquired and processed using the image acquisition processes in the flow chart. Figure 8A shows the background image (A) of the system while figure 8B shows cassava leaf sample with the background (B). The image in (A) was subtracted from image in (B) to get the image of the cassava leaf (C). When the edge algorithm was applied to image (C), image (D) was obtained. The image in (C) does not show any concentration of highlight intensities (specular component) on the leaf surface. Figure 9 shows the pixel histogram of the Red (R), Green (G) and Blue (B) colours from each of the leaves in Figure 7. There are significant differences in the R-, B- and G-pixel spectra of all the leaves implying the leaves are different and this qualitative information lends itself to discrimination algorithms using RGB. The Senescence leaf showed a very unique RGB pixel histogram depicting high pixel intensities for R and G and broader one for B. This could be attributed to the yellowish colour as yellow is a combination of Red and Green. This means that though the leaf appears yellowish to the human eye there is
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Figure 6: Correlation of area calculation using edge detected technique and histogram technique

Figure 7: Images of cassava leaves: (a) is the healthy green cassava leaf, (b) is the mildly infected mosaic cassava leaf, (c) is the severely infected mosaic cassava leaf and (d) a senescence cassava leaf.
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Figure 8: Example of image acquisition processes for cassava leaf: A – Background image; B - image of the cassava leaf with the background ; C - Processed Image:- Background image ( A) subtracted from image in ( B); D - Edge detected image of image (C).

a sizable amount of B in it. On the effect of the ACMD on the leaves we could see that due to the severity of the ACMD on the leaf (b) the G-pixel histogram shift is broader than most of the other G-pixel histograms. Also the frequency of the pixels (pixel counts) reduced compared to that of the healthy and mildly affected leaves. From the RGB-pixel histograms, the level of the effect of the disease lend itself to easy quantification using our developed matlab codes on the captured images by the system (see Figure 8).

DISCUSSION

A simple polarized-based diffuse reflectance imaging system, made up mainly of halogen lamp, web camera, which is relatively cheap, and linear polarizers has been built and demonstrated. The sample images acquired did not show any concentrated lube of highlight intensities (specular component) on the leaf surface, which normally produces erroneous images. Thus, there was no need for vision algorithms for scene segmentation. The cassava mosaic disease diagnostics demonstrated, provided valuable information about the status of the infected and uninfected leaf samples. The RGB spectral showed the difference between a diseased cassava leaves and that of a senescence cassava leaf.

Ghana, an agricultural based country, has many biological samples such as orange, watermelon, banana and pawpaw and they all have diseased
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<th></th>
<th>Red</th>
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<th>Blue</th>
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<tr>
<td><strong>Background</strong></td>
<td><img src="image1.png" alt="Histogram" /></td>
<td><img src="image2.png" alt="Histogram" /></td>
<td><img src="image3.png" alt="Histogram" /></td>
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<tr>
<td><strong>Healthy Leaf</strong> <em>(a)</em></td>
<td><img src="image1.png" alt="Histogram" /></td>
<td><img src="image2.png" alt="Histogram" /></td>
<td><img src="image3.png" alt="Histogram" /></td>
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<tr>
<td><strong>Mildly Infected Leaf</strong> <em>(b)</em></td>
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<td><img src="image2.png" alt="Histogram" /></td>
<td><img src="image3.png" alt="Histogram" /></td>
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<tr>
<td><strong>Severely Infected Leaf</strong> <em>(c)</em></td>
<td><img src="image1.png" alt="Histogram" /></td>
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<tr>
<td><strong>Senescence Leaf</strong> <em>(d)</em></td>
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<td><img src="image2.png" alt="Histogram" /></td>
<td><img src="image3.png" alt="Histogram" /></td>
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Figure 9: RGB-pixel histogram of various leaves in figure 7: a) background, b) severely infected CMD leaf c) healthy cassava leaf, d) mildly infected CMD leaf and d) senescence cassava leaf image
related problems with their leaves, for which this system can be used as a search tool. The web-cam can readily be replaced with an advance web-cam that can record other wavelengths with corresponding light source. The light source in the present system is somewhat not evenly distributed, leading to image correction. However, an evenly distributed light source can be used.

Using other analytic techniques, such as multivariate image analysis (Gonzalez et al., 2004; Esbensen et al., 1994) this system can be used for application in medical and biological diagnostics as well as in food science where detection of complex samples is required for quantification using imaging.

While this system is not yet a replacement for sophisticated imagers, it is an attractive tool due to its simplicity, versatility, and low cost. In general, this imager can be a valuable tool for teaching and research in applied optics.

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REFERENCES


Doornbos, R. M. P., R. Lang, M. C. Aalders, F. W. Cross, and H. J. C. M. Sterenborg. (1999). The determination of in vivo human tissue optical properties and absolute chromophore concentrations using spatially resolved steady-state diffuse reflect-
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Matlab, 7.10.0 (2010). R2010a, Mathworks Inc. USA.


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